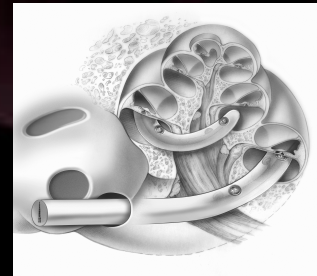
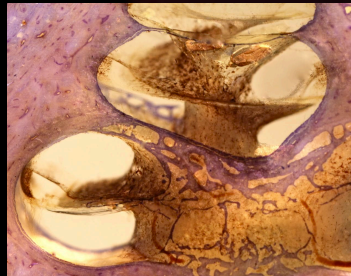
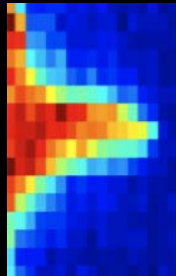




# Improved Outcomes with Cochlear Implants: Electrode Design, Surgical Methods

Stephen Rebscher

Epstein Laboratory  
University of California, San Francisco



# Major Collaborators:

Dr. Patricia Leake, UCSF

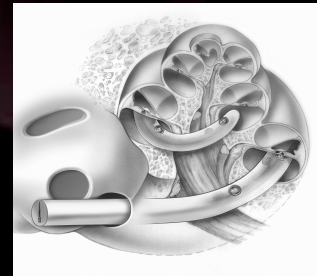
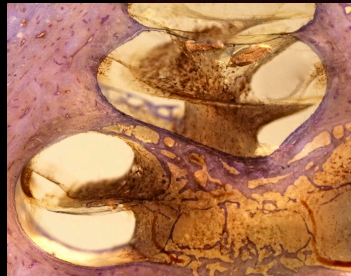
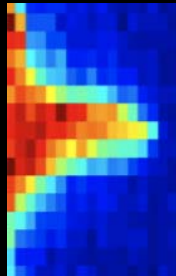
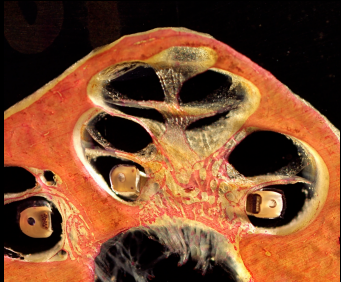
Dr. Russel Snyder, UCSF

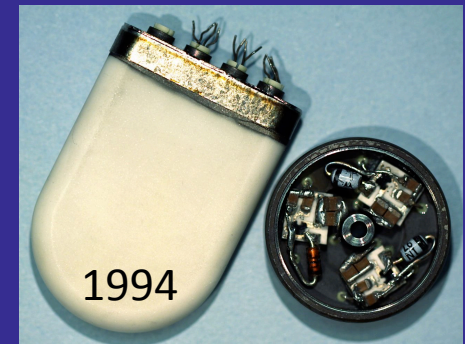
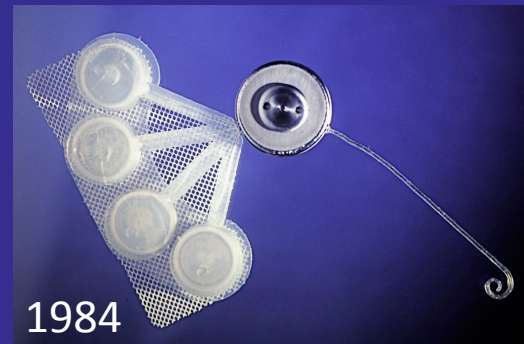
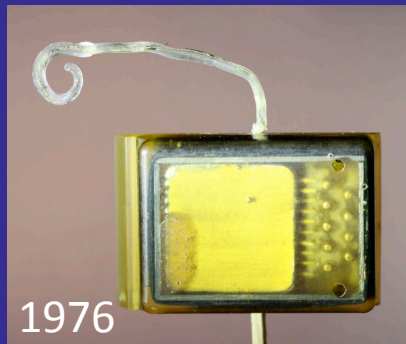
Dr. Larry Lustig, Columbia Univ.

Dr. J.T. Roland, NYU

Dr. William Luxford, HEI, USC

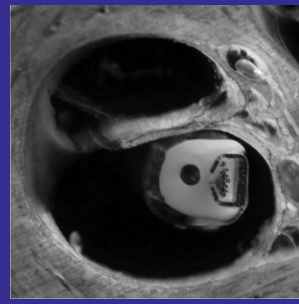
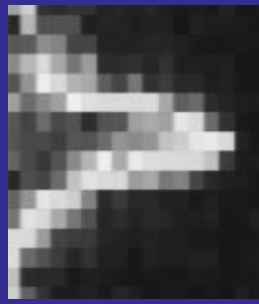
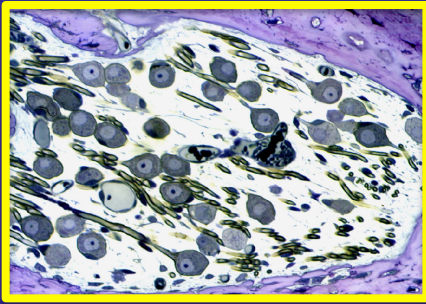
Dr. Peter Wardrop, Scottish Nat. CI Center



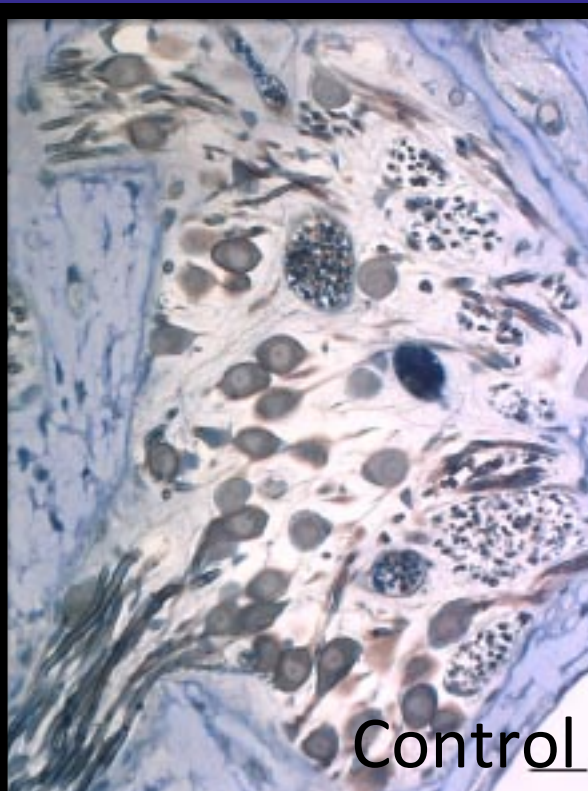
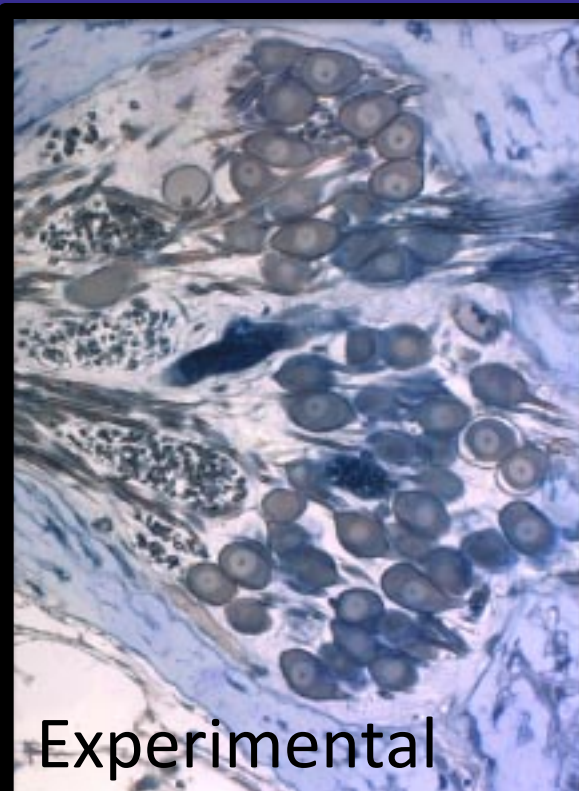


# History of Cochlear Implant Research at UCSF

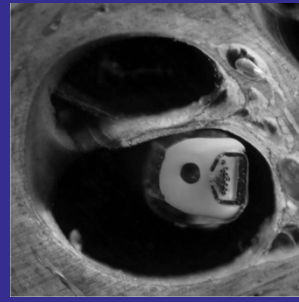
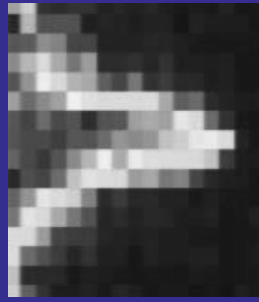
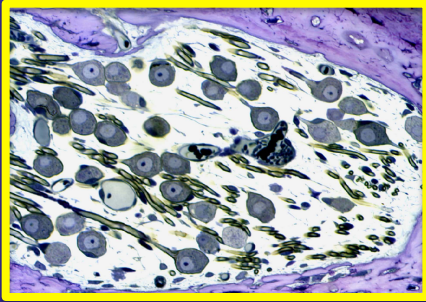
1. Early multichannel CI, 1970s, Dr. Robin Michelson
2. Chinese clinical exchanges began in 1970s
3. Electrophysiology, Dr. Michael Merzenich, F. and D. Russ Award, National Academy of Engineering, 2014
4. Safety of CI, Dr. R. Schindler, Dr. P. Leake
5. Multichannel clinical trials 1981
6. CI engineering lab at Peking Union Hospital, Dr. Z. Wang
7. IP transfer and clinical trials, Advanced Bionics 1990s
8. Nurotron Biotechnology shared development



Current Studies:  
Neural Survival



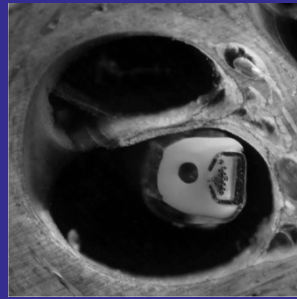
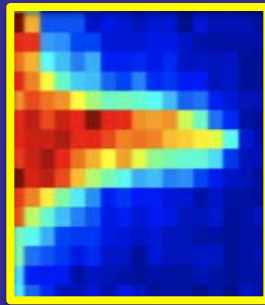
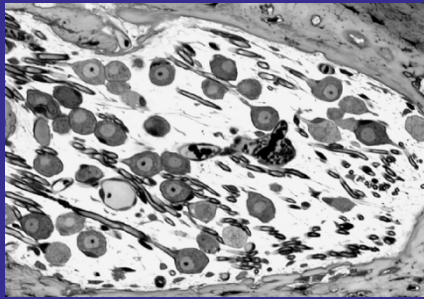
Ganglion cell survival



Current Studies:  
Neural Survival

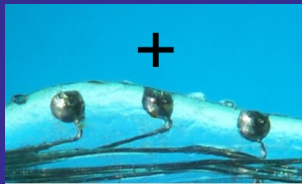
Long-Term Studies have shown:

1. Electrical stimulation has protective effect in SG
2. BDNF supports SG survival –osmotic pump or viral
3. Trauma degrades function

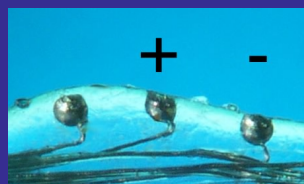


# Current Studies: Electrophysiology

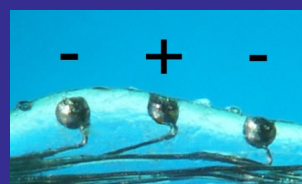
**Monopolar**



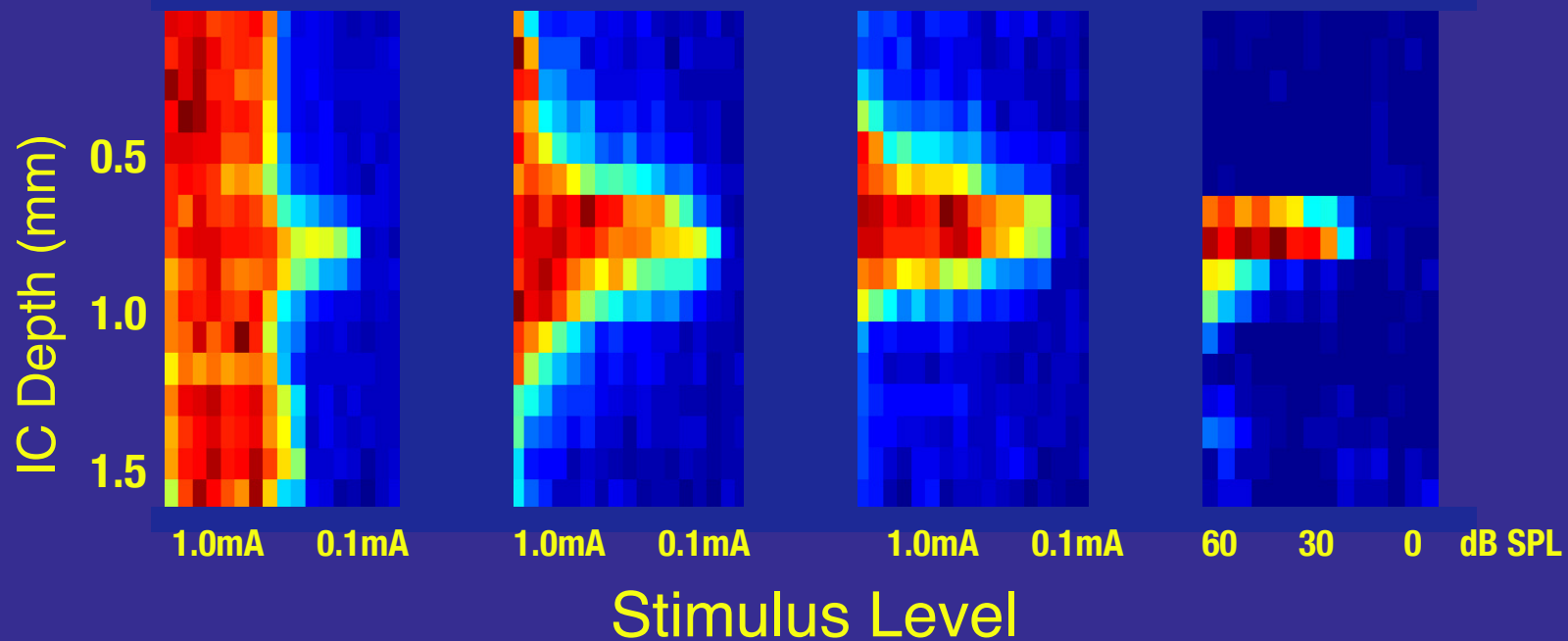
**Bipolar**

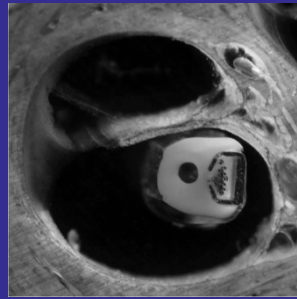
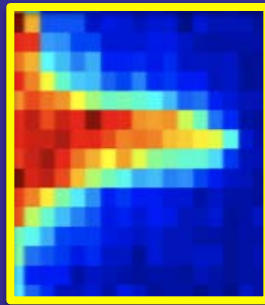
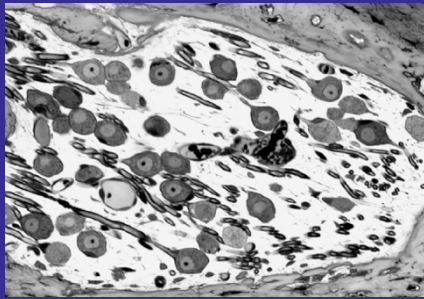


**Tripolar**



**Acoustic**

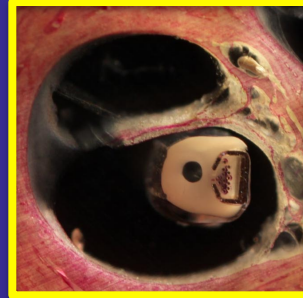
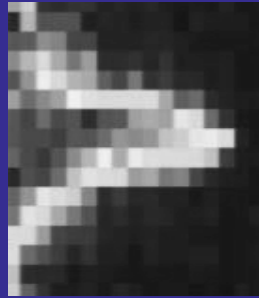
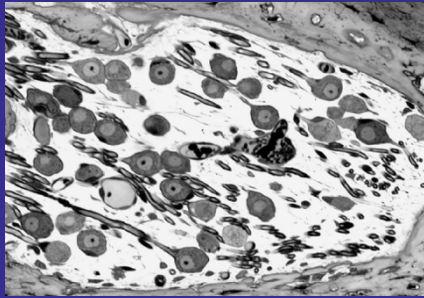




## Current Studies: Electrophysiology

Electrophysiology Studies have shown:

1. Central responses to E-stim can be very localized  
Monopolar – Bipolar – Tripolar
2. Chronic E-stimulation maintains tonotopic tuning
3. Chronic E-stimulation helps to maintain firing rate
4. Loss of spiral ganglion degrades function

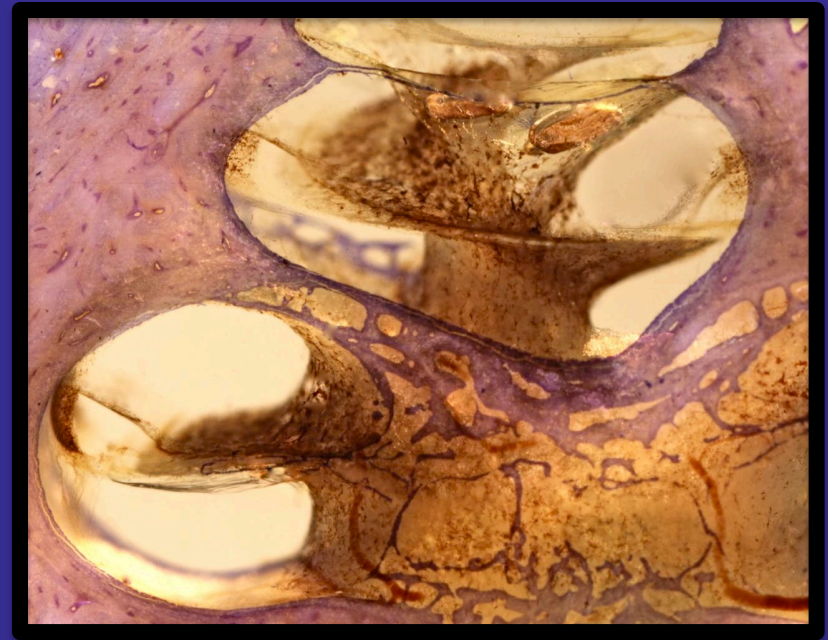


## Current Studies: Insertion Trauma

# *Temporal Bone Studies*

## *Purpose:*

*To evaluate the role of mechanical stiffness, electrode size and electrode shape in insertion trauma*



## *Manufacturers:*

*Advanced Bionics LLC, USA*

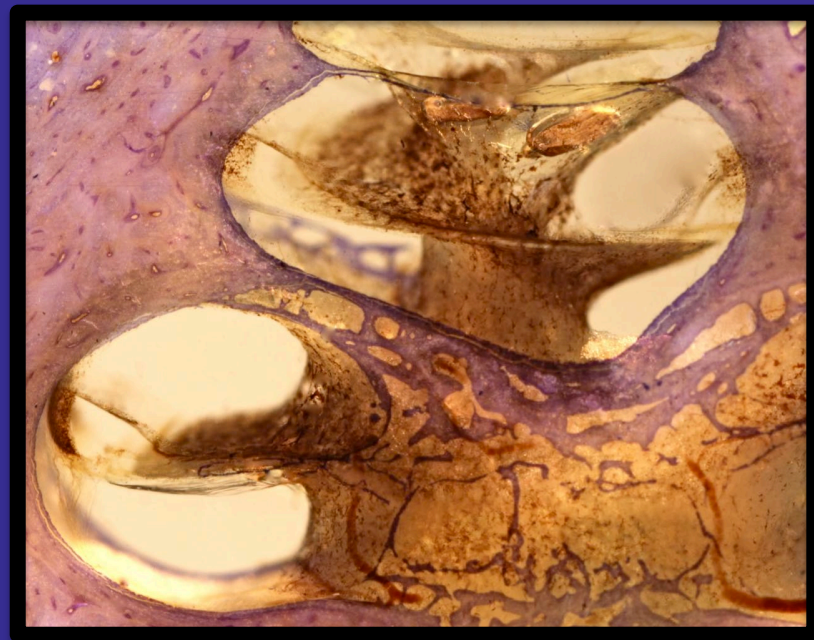
*Cochlear Corporation, Australia*

*Nurobiosis, Seoul, South Korea*

*Nurotron Biotechnology, China*

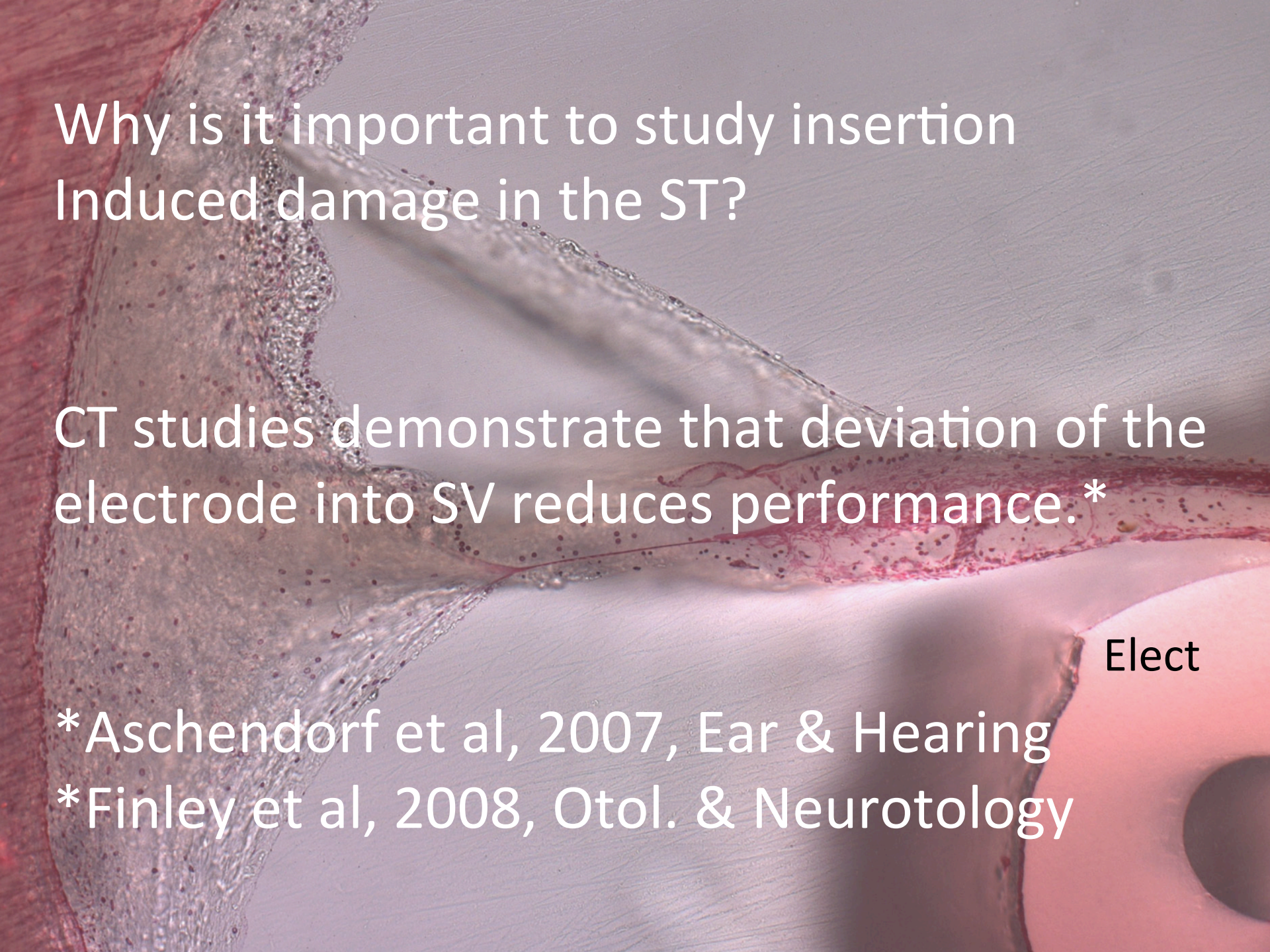
## *Electrodes Studied:*

*Cochlear Banded - Cochlear Contour -  
Contour Advance - AB Spiral –  
AB HiFocus II w/ POS - AB HiFocus 1j  
AB Prototype Lateral Wall (3) –  
Nurotron CS10A – Nurobiosis  
N= 9/166*



## *Participating Surgeons (n=19):*

Dr. A. Eshraghi, USA – Dr. Fu Yong, China – Dr. Haynes, USA  
Dr. Hu Baohua, China - Dr. Labbadie, USA – Dr. T. Lenarz, Germany  
Dr. Li Jianan, China – Dr. L. Lustig, USA – Dr. W. Luxford, USA  
Dr. Manrique, Spain - Dr. Peng Shaopeng, China – Dr. Rivas, USA  
Dr. J.T. Roland, New York – Dr. Shi Ziquang, China  
Dr. W. Slattery, USA – Dr. Sun Shuping, China – Dr. Wanna, USA  
Dr. David Whinney, UK - Dr. Peter Wardrop, Scotland

A microscopic image of a cochlea, showing the spiral ganglion and the cochlear duct. An electrode array is visible, inserted into the cochlear duct. The electrode array is a long, thin, curved structure with small electrodes at the end. The cochlear duct is a large, clear, fluid-filled space. The spiral ganglion is a cluster of cells located near the base of the cochlea. The electrode array is positioned such that it is in contact with the cochlear duct, but not with the spiral ganglion. The electrode array is labeled "Elect" in the bottom right corner.

Why is it important to study insertion  
Induced damage in the ST?

CT studies demonstrate that deviation of the  
electrode into SV reduces performance.\*

Elect

\*Aschendorf et al, 2007, Ear & Hearing

\*Finley et al, 2008, Otol. & Neurotology

- physically damaged, neural loss
- distorted frequency mapping
- shallow insertion



## Intracochlear Damage

- high thresholds
- poor DR
- high channel interaction

SV

Perilymph (High  $\text{Na}^+$ , Low  $\text{K}^+$ )

RM

SM

Endolymph (Low  $\text{Na}^+$ , High  $\text{K}^+$ )

Sp Gang

OSL

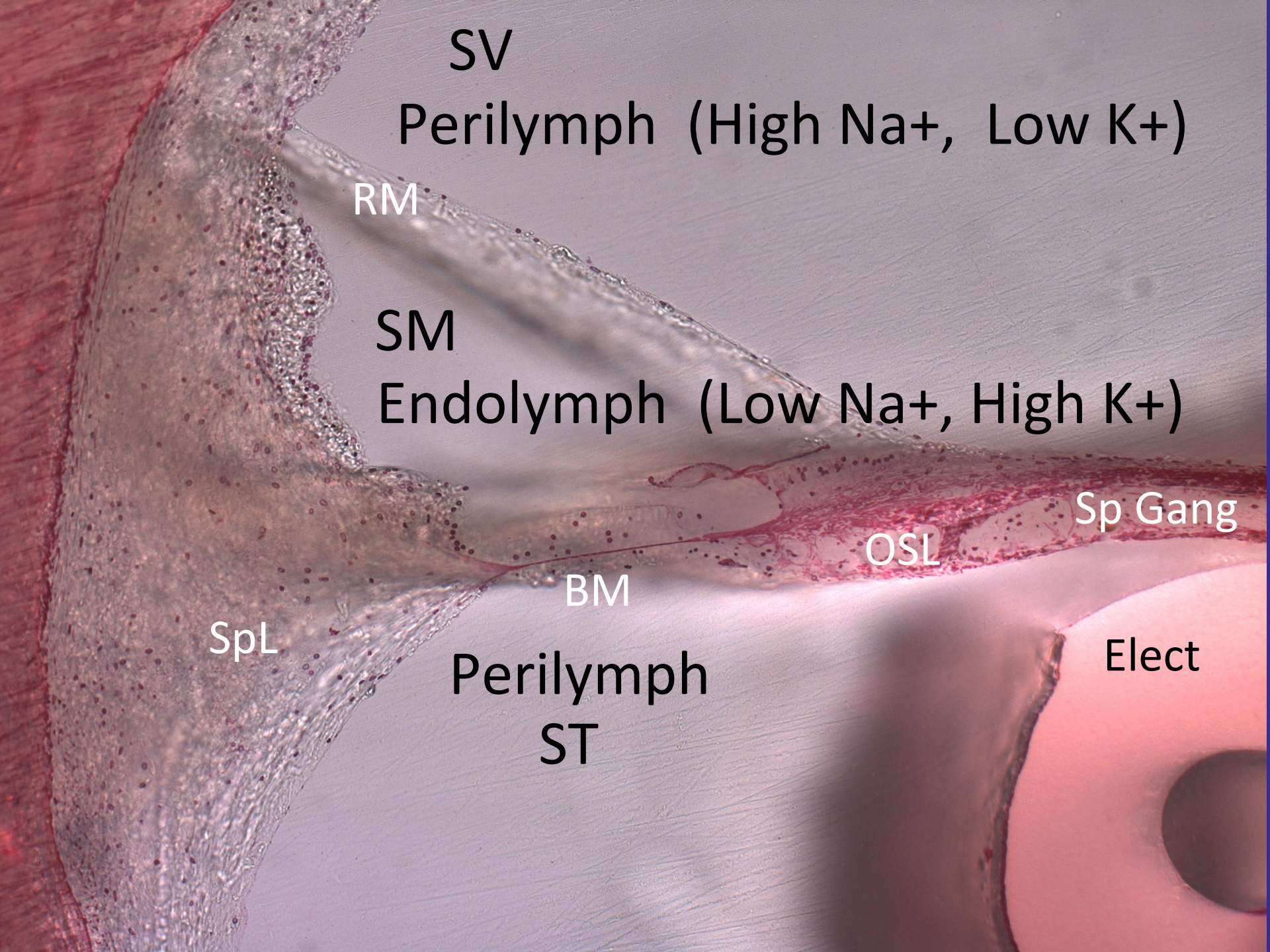
BM

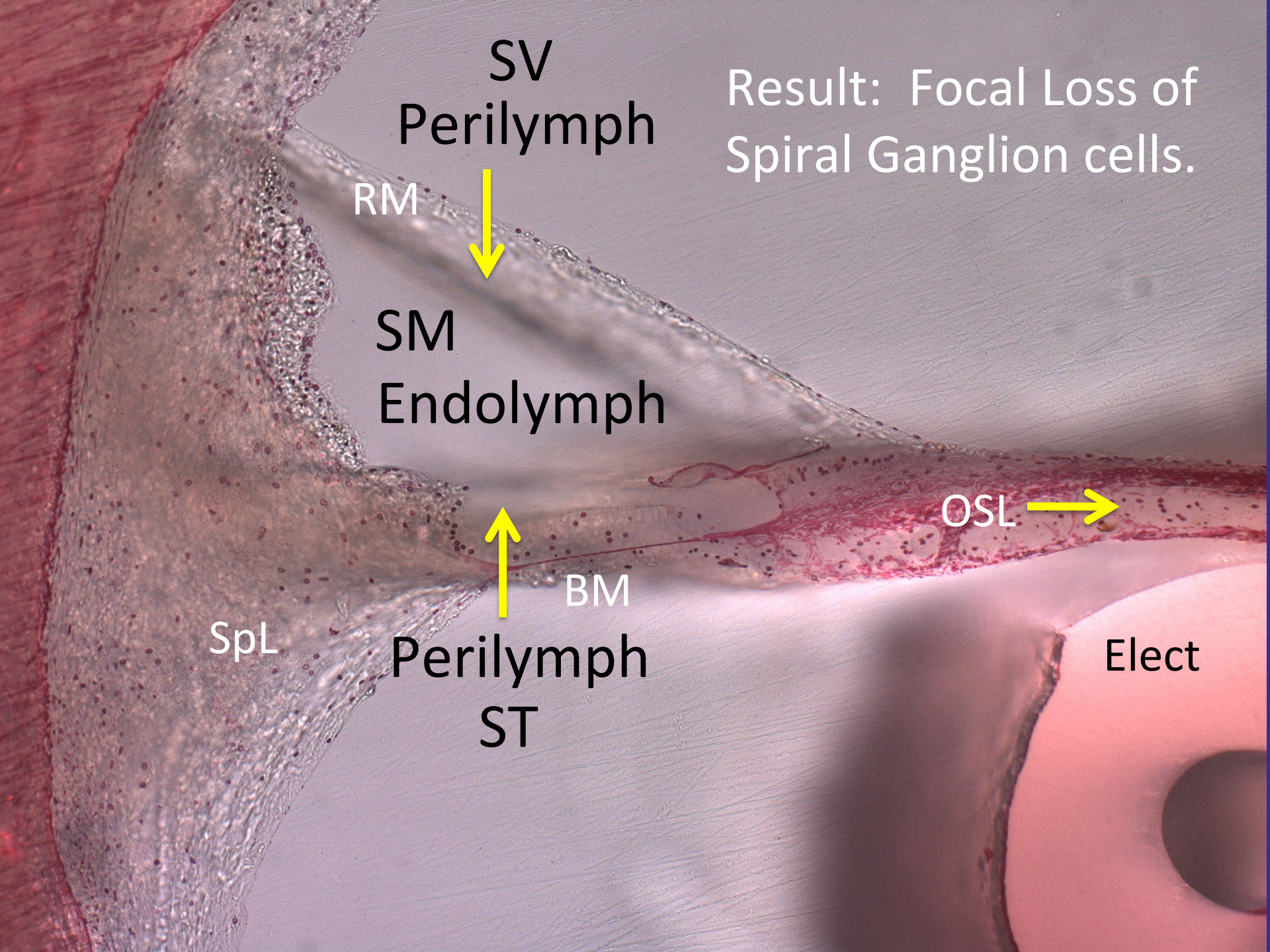
SpL

Perilymph

ST

Elect





Result: Focal Loss of  
Spiral Ganglion cells.

SV  
Perilymph

RM

SM  
Endolymph

OSL

BM

SpL

Perilymph  
ST

Elect

# Reduction in electrode size over time

1980-90s

1990-10s

2010-current

n=35

Cochlear Contour

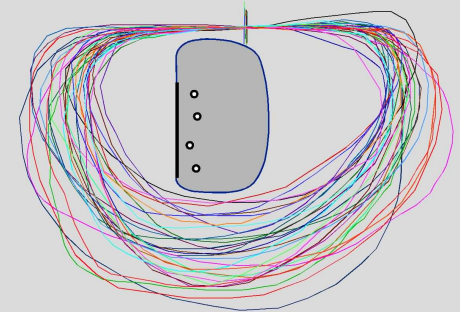
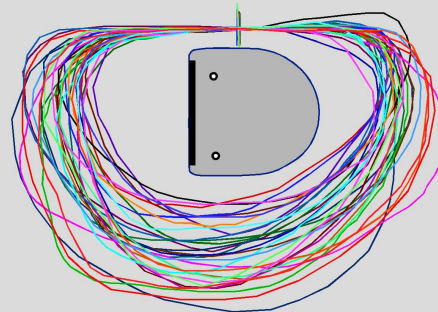
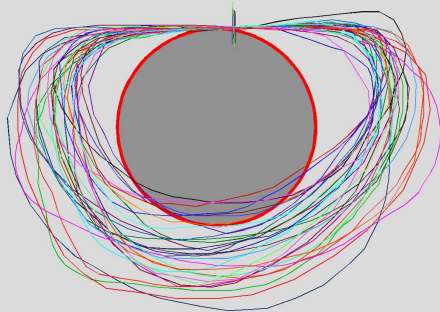
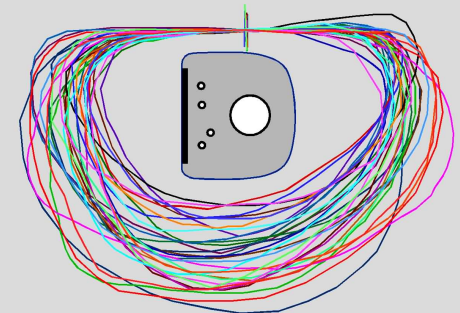
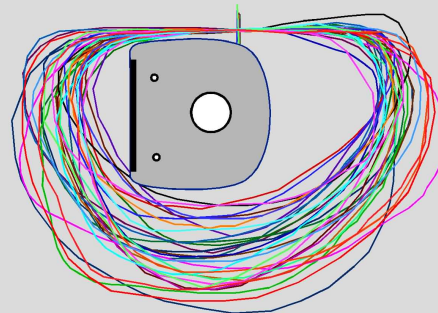
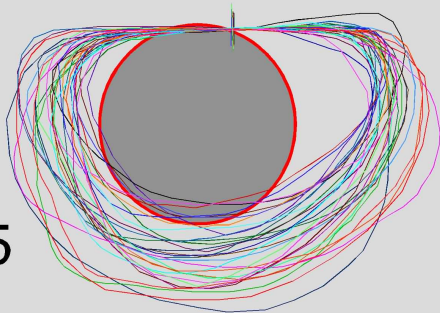
Helix

HF Mid Scala

Adv. Bionics Spiral  
330° 1.0 mm

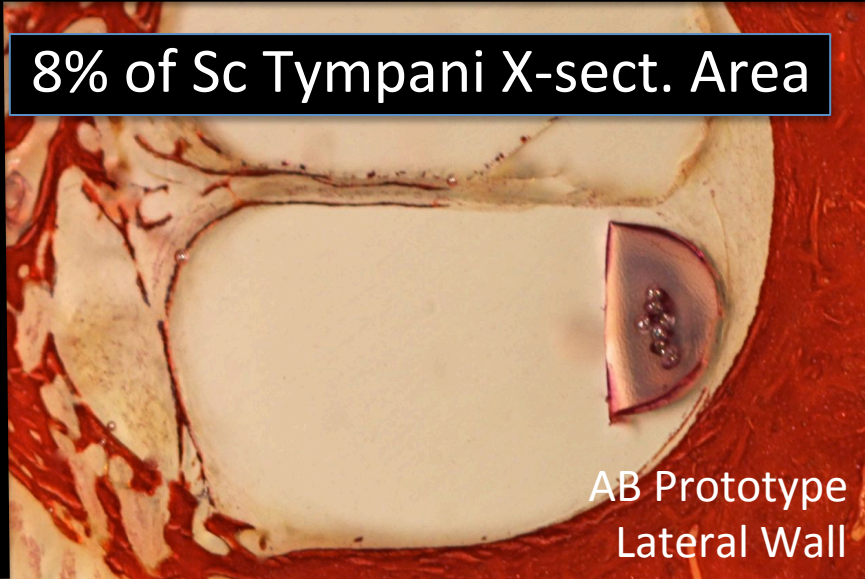
HF Ij

Nurotron CS10A



# Current Examples

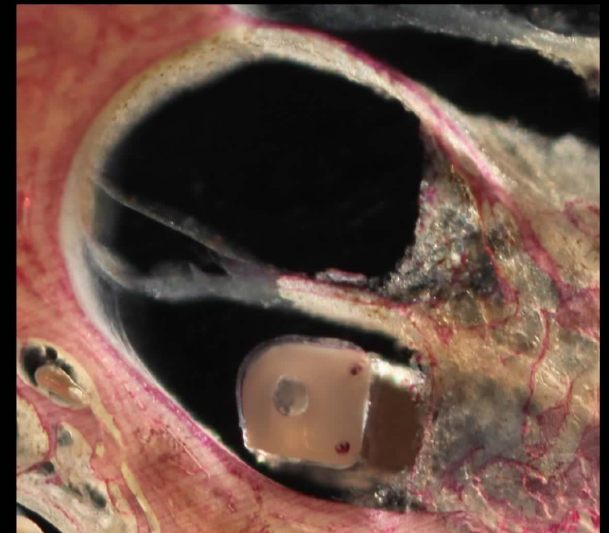
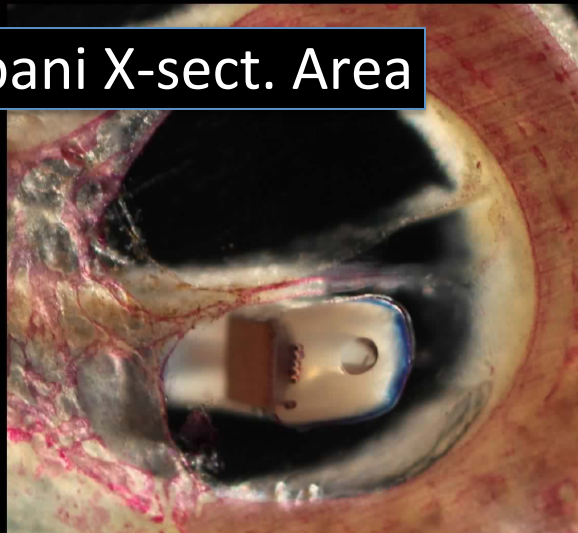
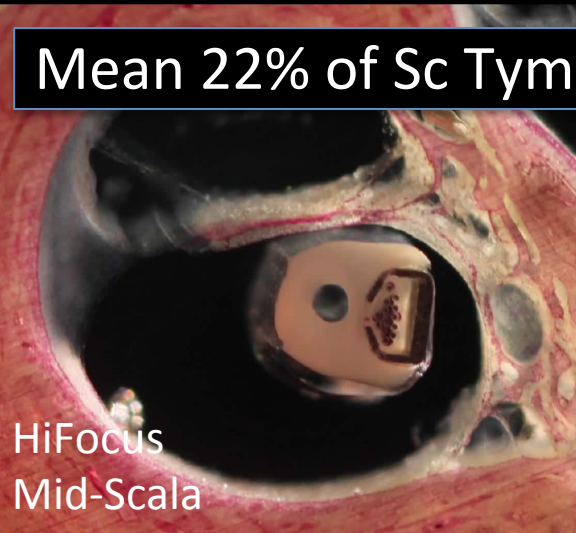
8% of Sc Tympani X-sect. Area



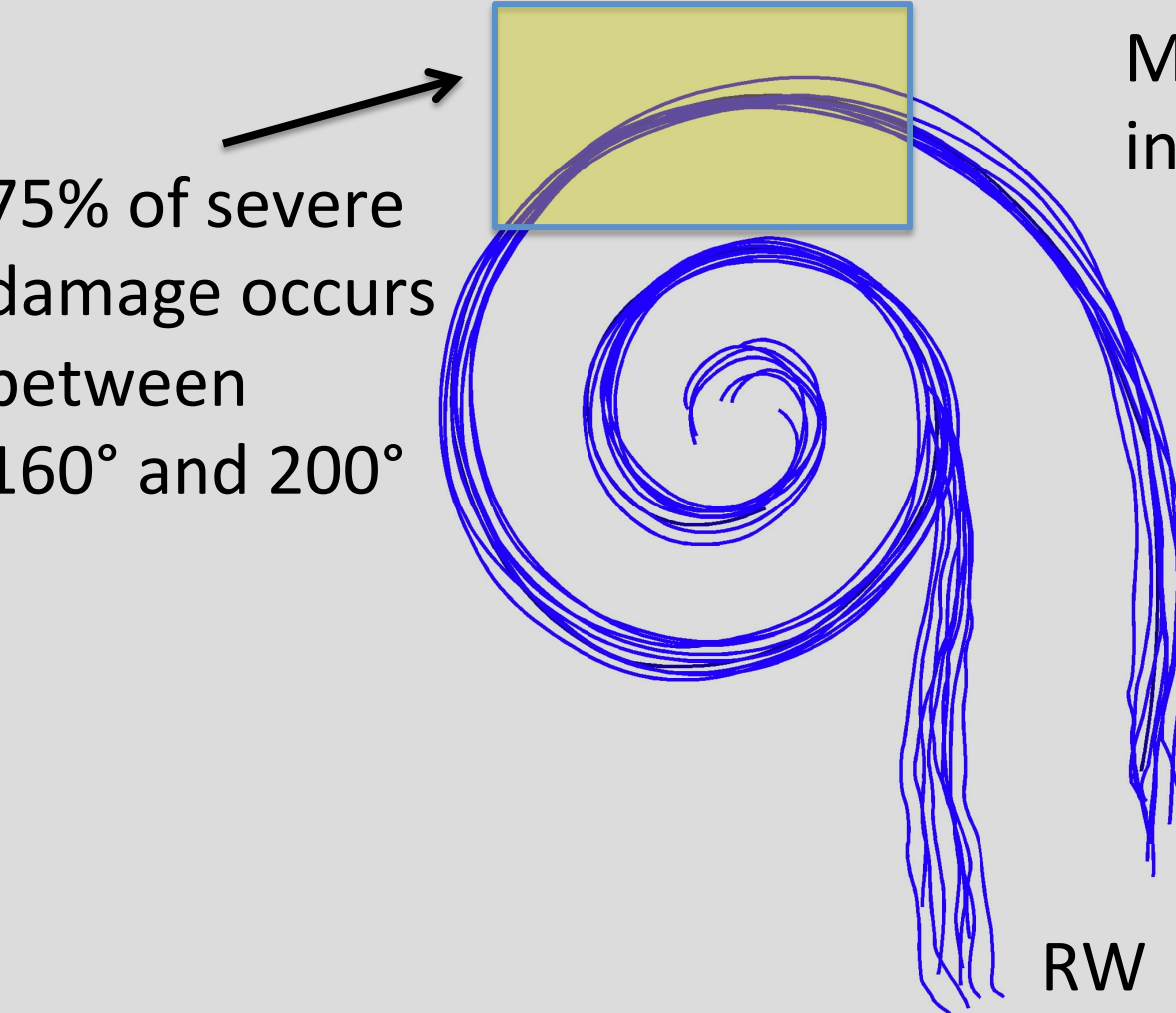
12% of Sc Tympani X-sect. Area



Mean 22% of Sc Tympani X-sect. Area



Where, and how, does damage most often occur?



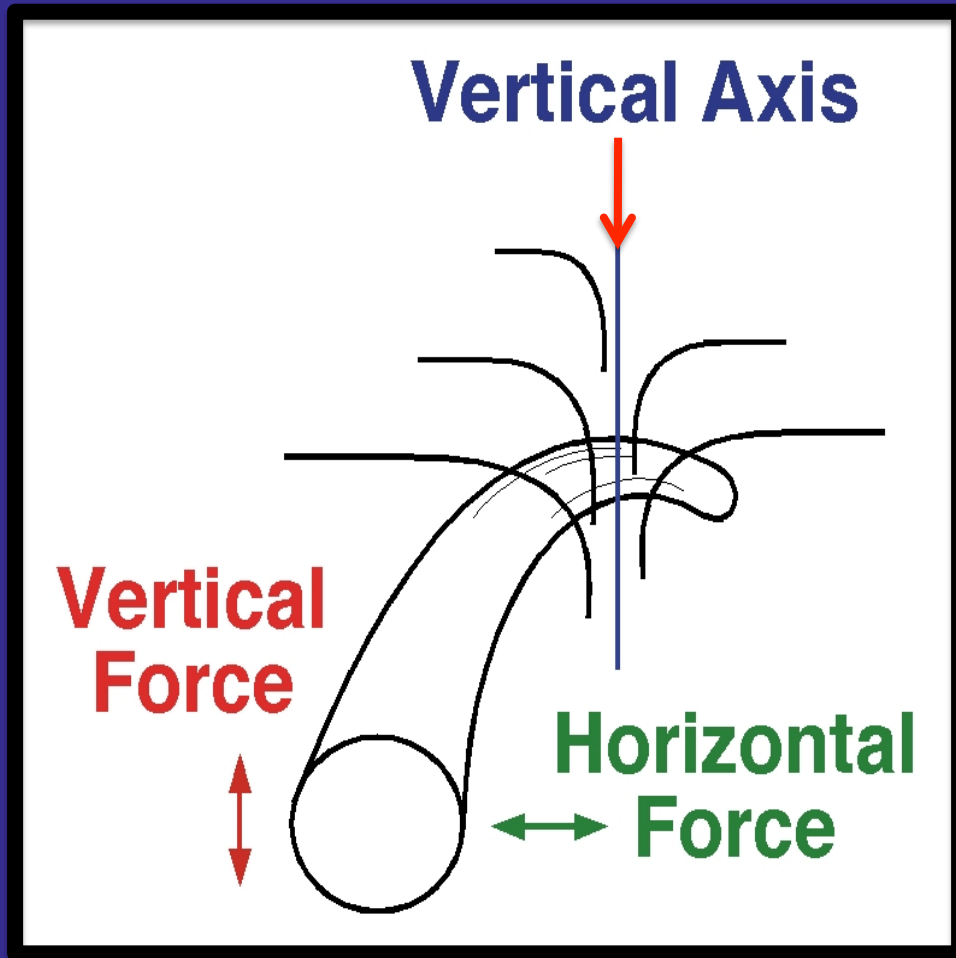
Mean Location of deviation into Sc. Vest. 181° from RW



# How do mechanical properties effect the rate of trauma?

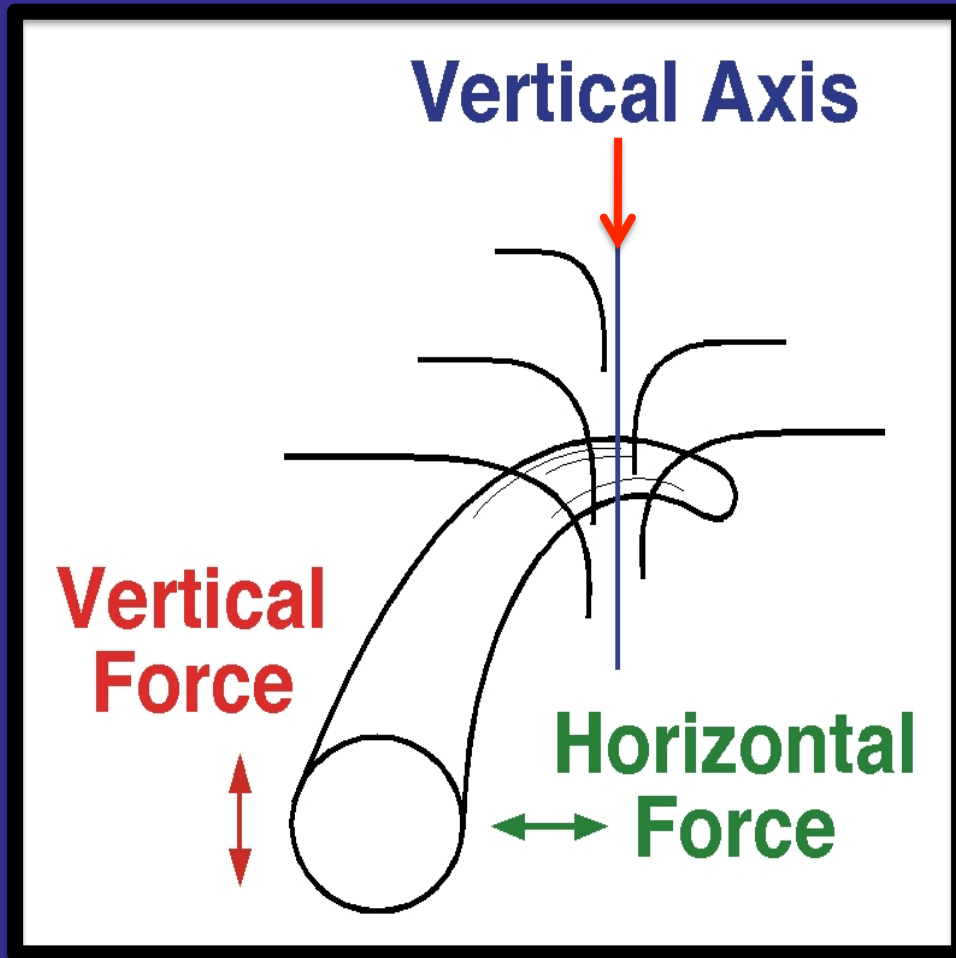
We hypothesize that an electrode which is more stiff in the vertical plane will be less likely to deviate from the scala tympani upward in to the scala vestibuli.

To test this hypothesis we measured:



1. The vertical and horizontal stiffness of each electrode design.

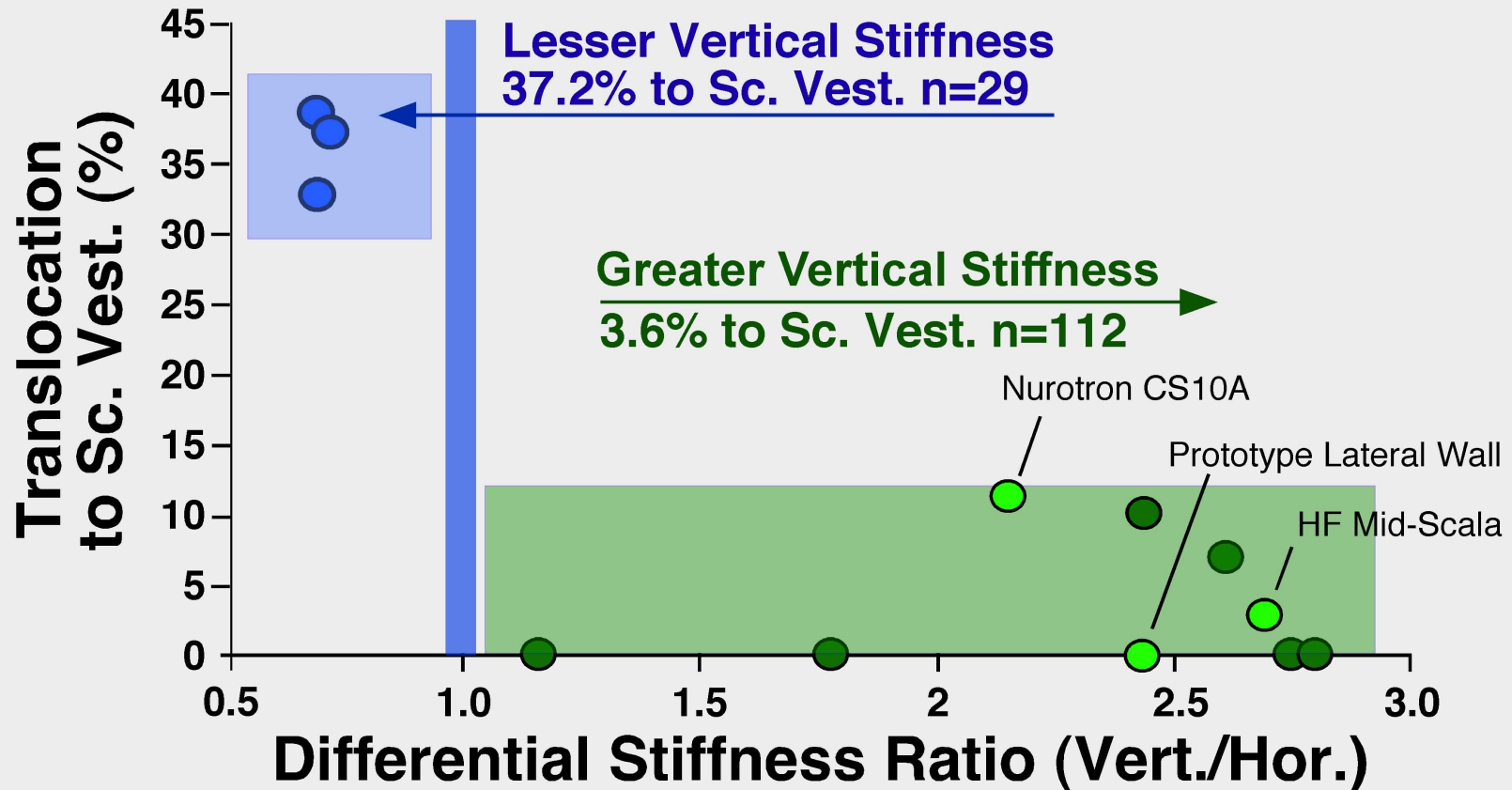
To test this hypothesis we measured:



2. Correlated with the incidence of trauma observed with each design.

# Vertical stiffness effects the rate of trauma

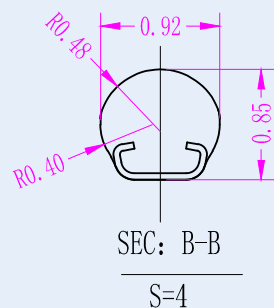
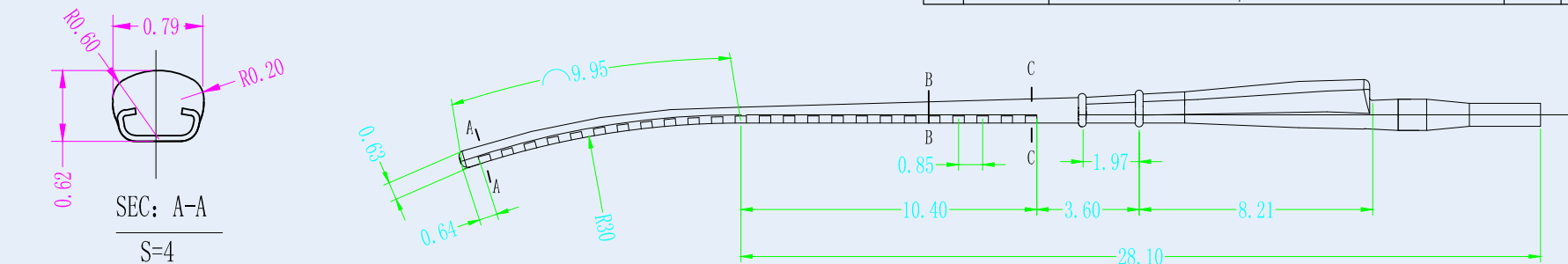
HF II POS >400° ●



SHALL NOT BE DISCLOSED, DUPLICATED WITHOUT THE PRIOR WRITTEN PERMISSION OF NUROTRON

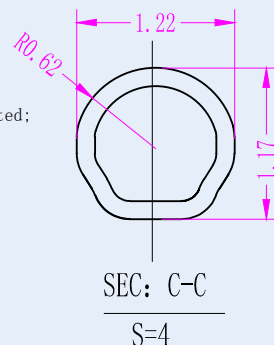
A4

Change record				
REV.	ECN	Description	Date	name
1		First issue	2012/08/05	paul
2	E0000595	Change Tolerance	2013/08/05	paul
3		The replacement of the frame	2015/09/29	paul





NOTE:

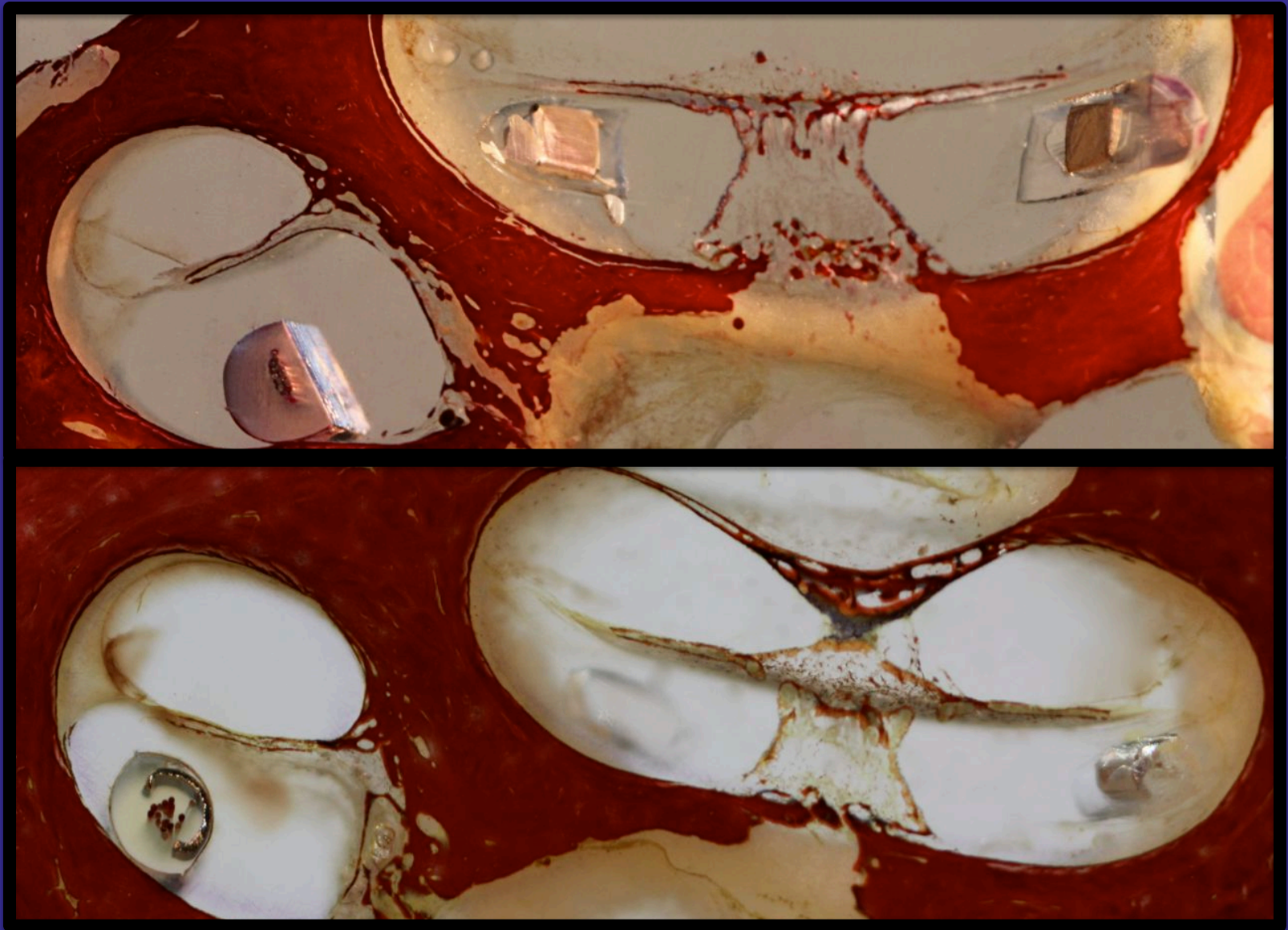
1. Please check 3D diagram if dimension not indicated;
2. EL array length:  $20.5 \pm 0.25\text{mm}$ ;
3. Pitch of contacts:  $0.85 \pm 0.1\text{mm}$ ;
4. Number of contacts: 24PCS
5. All of the tolerance within  $\pm 0.05\text{mm}$ ;



## 24, 20, 16 mm Lengths Smaller Profile

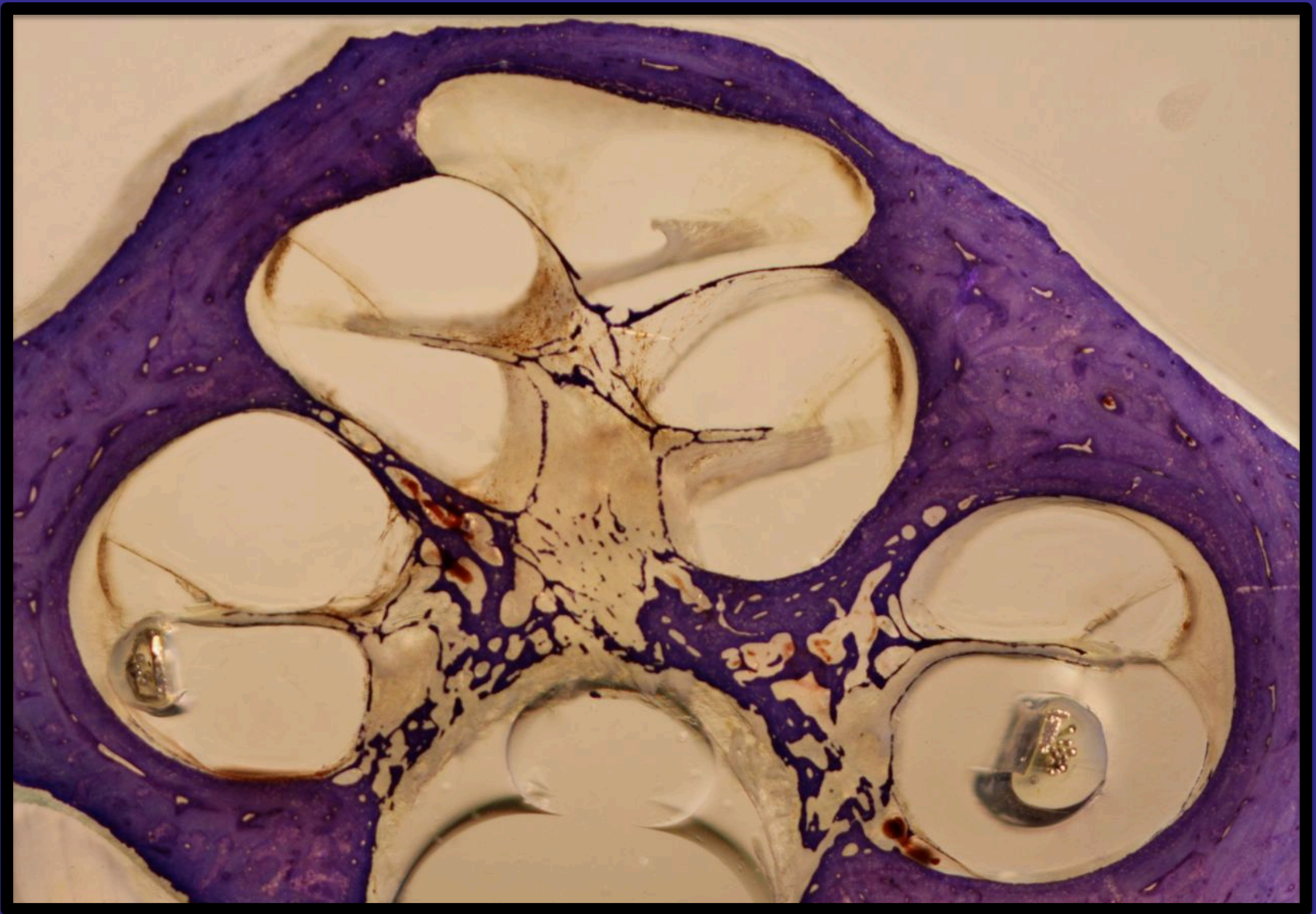
2		Silica:MED-4244				YL00.0001
1	CS4.010.100	Contact with wire (72)			24	EL injection
N0:	Drawing number	Description			Number	Remarks
Tolerance: X.X    ±0.15 X.X X   ±0.10 X.XXX   ±0.05  Angle tolerance: ±2°		<div>NUROTRON</div> <div>诺 尔 康</div>		浙江诺尔康神经电子科技股份有限公司		
				ZheJiang Nurotron Biotechnology Co., LTD		
			Name	Date	DESCRIPTION: EL CS-10A(DS)	Scale
	DRAWN	Zhiping tan	2015/09/29	DEVICE: CS-10A	REV.	3
 		CHECKED	See Agile	DWG NO: CS4.010.104		SHEET 1 OF 2
		ENG APPRI	See Agile	Material: : NA		Unit: mm

Electrodes stiffer in the vertical plane seldom deviate to Sc V



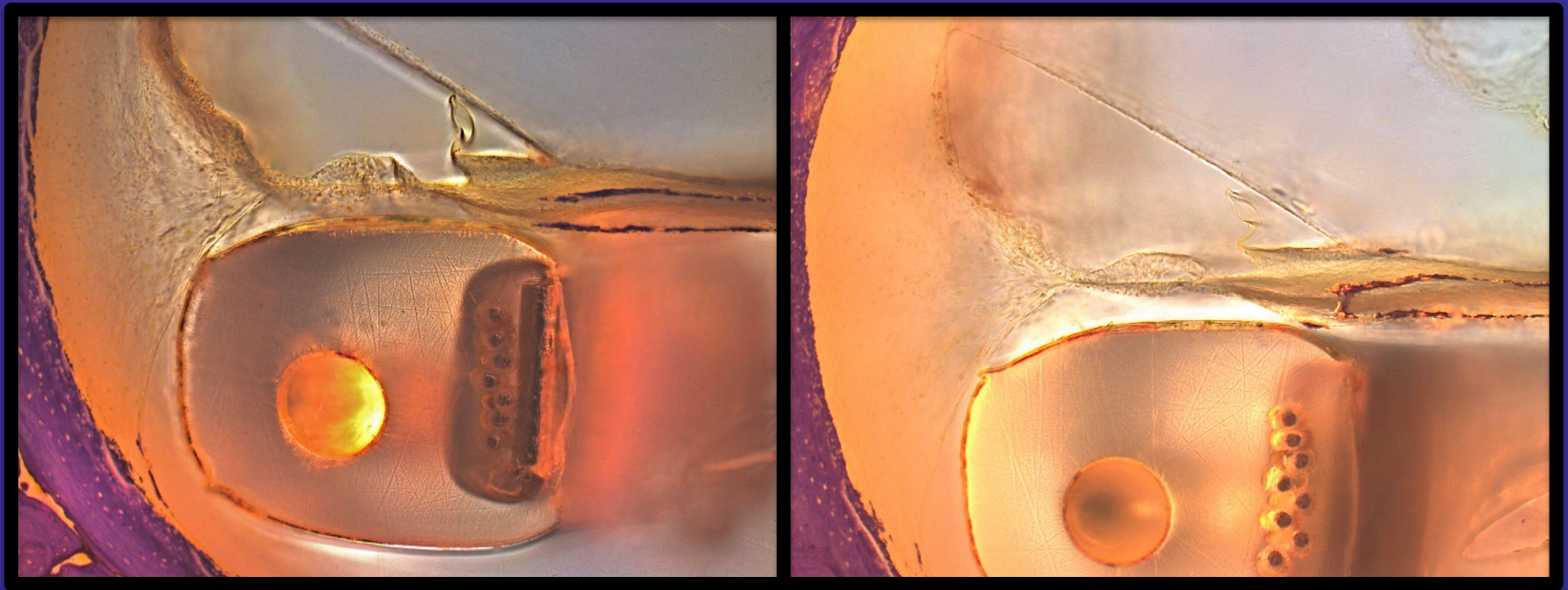
Nurotron CS10A

Straight arrays are located more lateral in the upper turns

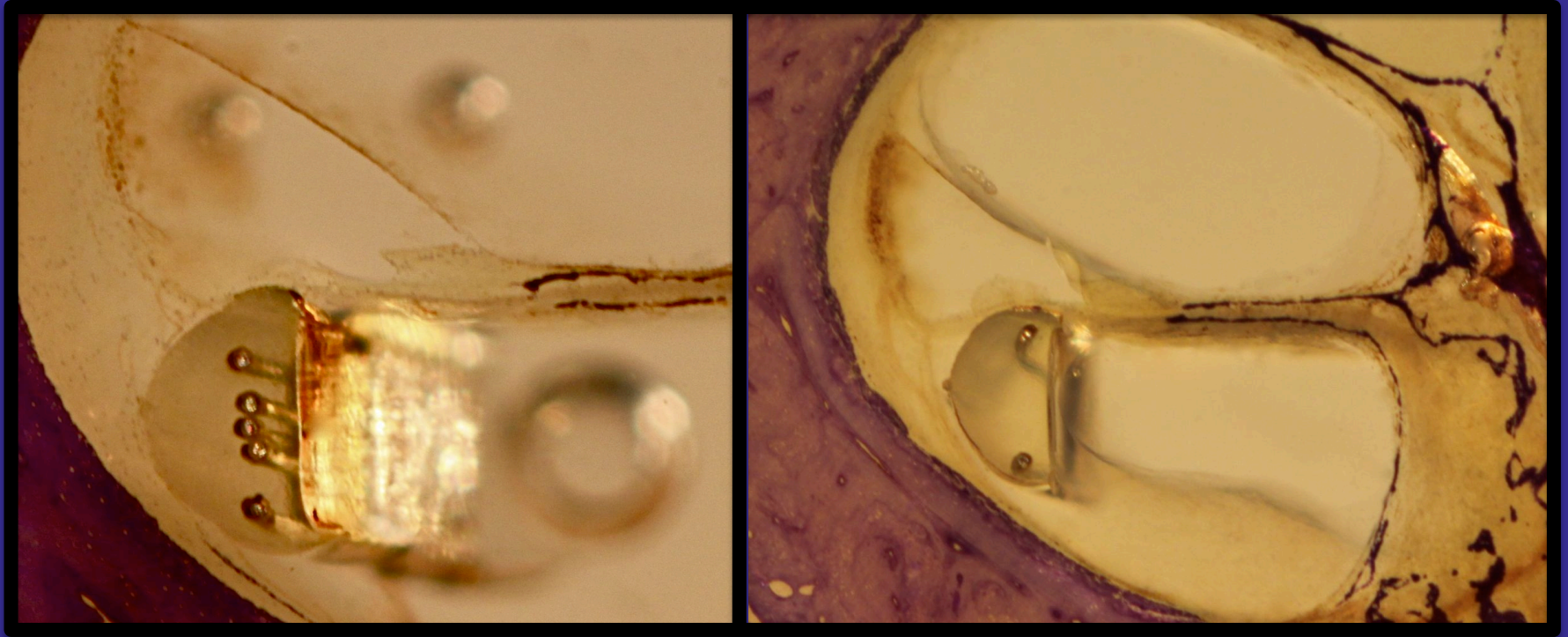


AB Lateral Wall Prototype

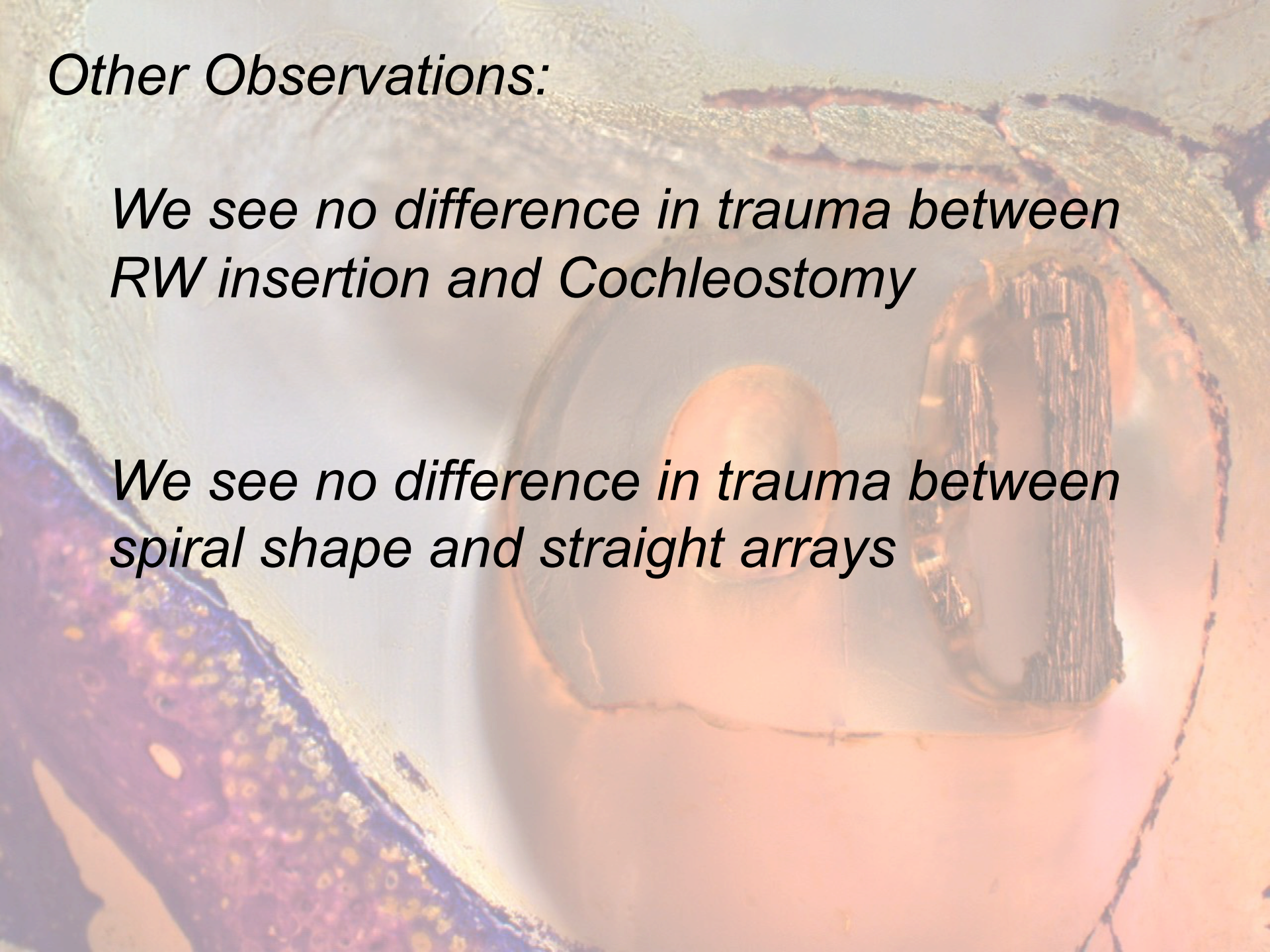
Lateral located electrodes may contact the Sp Ligament or Basilar membrane, in many cases without damage.



When distortion is observed it is most often minimal (Eshraghi Scale = grade 1), particularly with arrays that are stiffened in the vertical plane.



The effect of this distortion on residual hearing is unknown.

A microscopic image of cochlear tissue, showing a spiral-shaped electrode array (RW) inserted into the cochlea. The array is visible as a dark, textured structure within the cochlear duct. The surrounding tissue is stained, showing various cellular structures and the overall spiral shape of the cochlea.

## *Other Observations:*

*We see no difference in trauma between  
RW insertion and Cochleostomy*

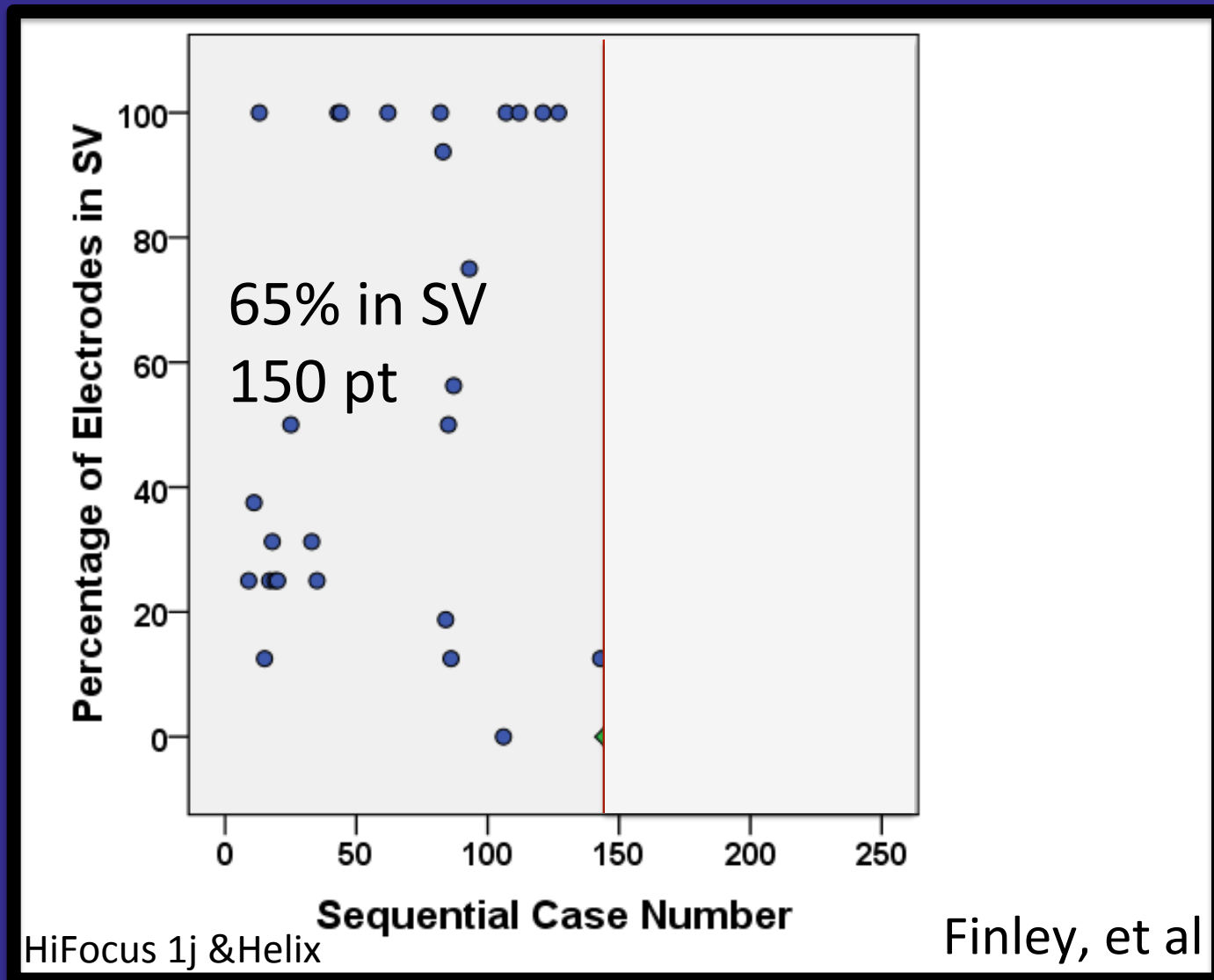
*We see no difference in trauma between  
spiral shape and straight arrays*

Do these improvements, i.e. reduced size and increased vertical stiffness, mean we will no longer see intracochlear trauma?

Do these improvements, i.e. reduced size and increased vertical stiffness, mean we will no longer see intracochlear trauma?

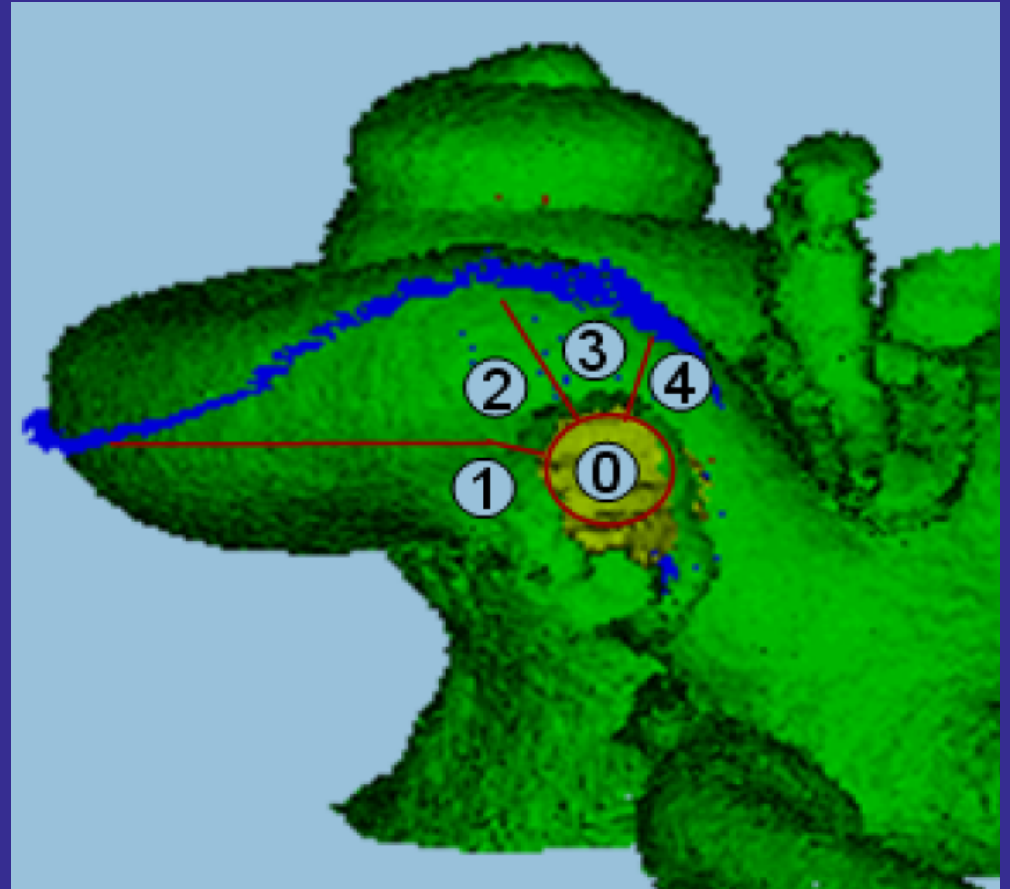
Unfortunately, the answer is “No”

# Surgical technique can strongly affect the rate of trauma

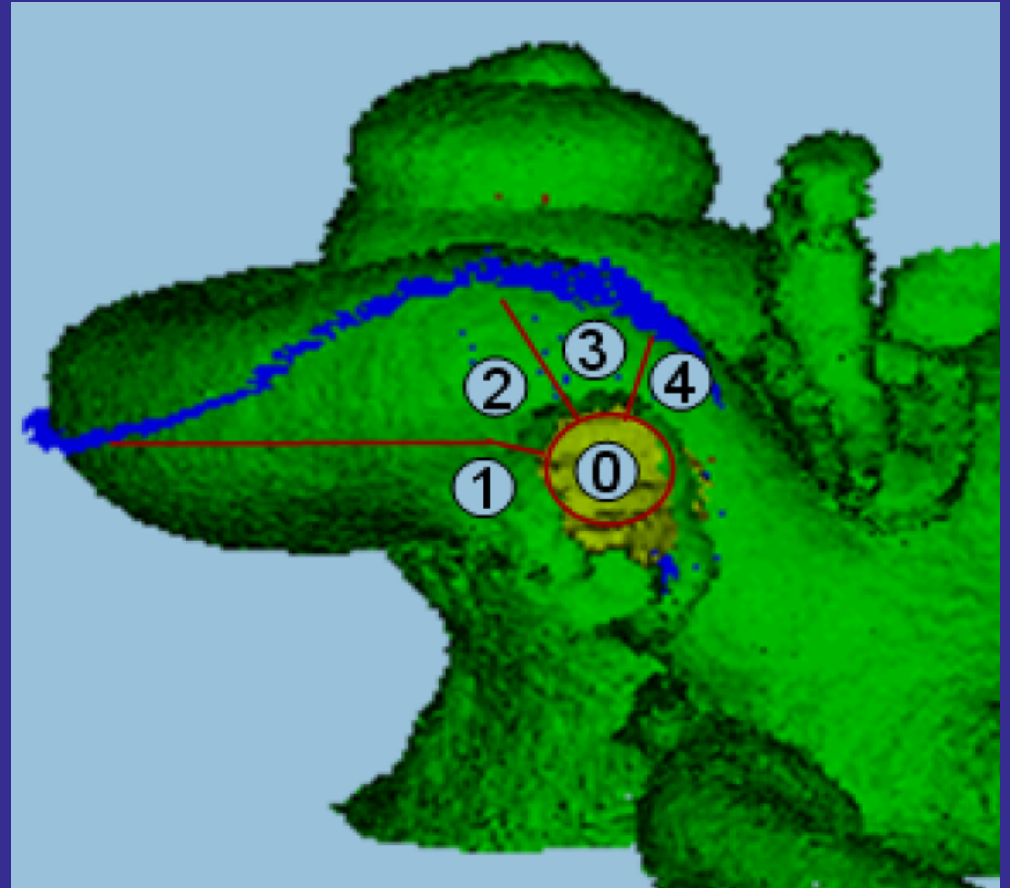


\*6 other studies averaged 4.5% in SV, same arrays

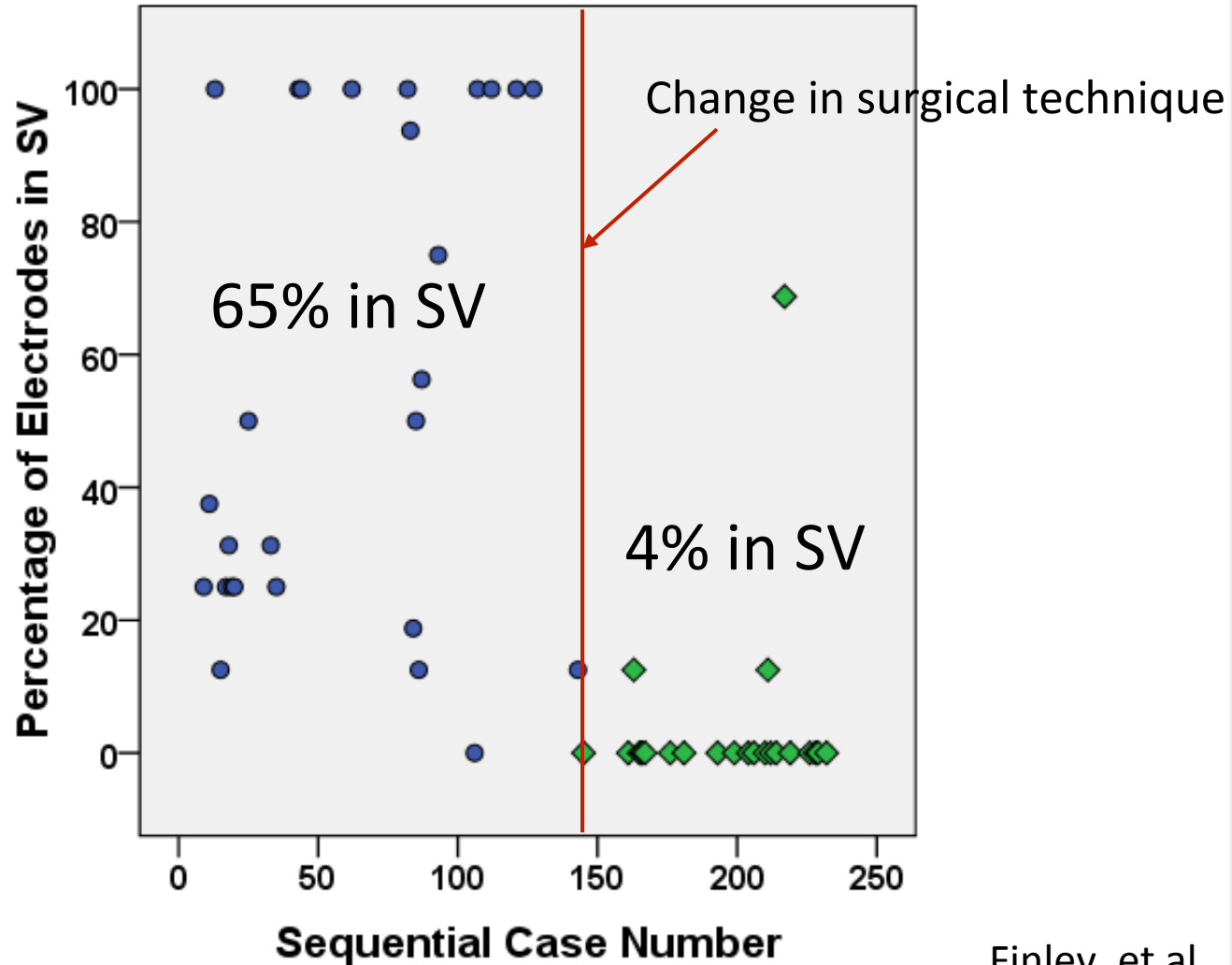
Does cochleostomy  
location affect the  
percentage of electrodes  
in Scala Vestibuli?



What would happen if the surgeon made a concerted effort to place all cochleostomies in region #1?

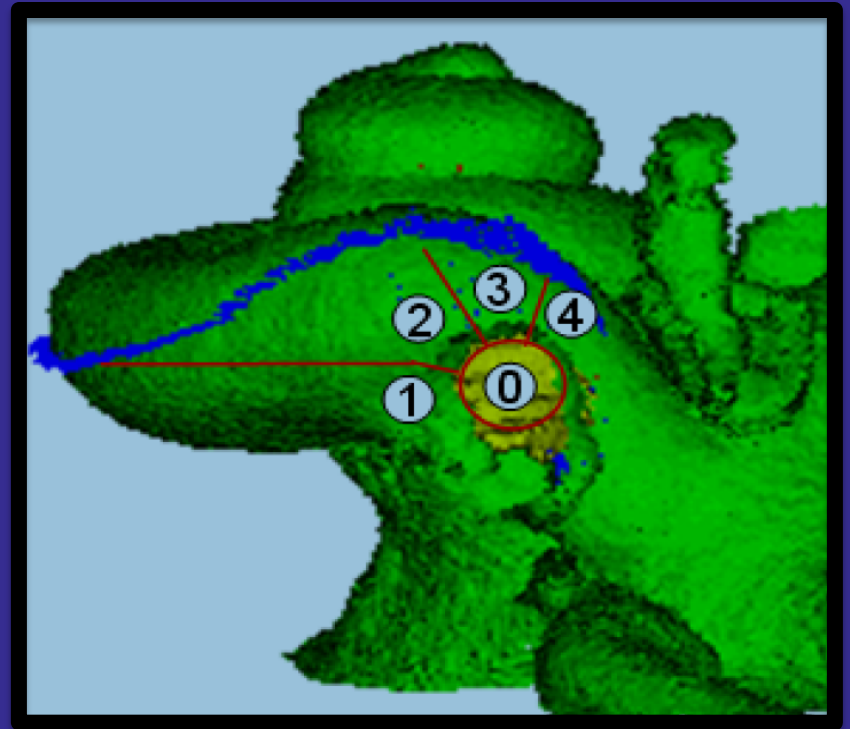
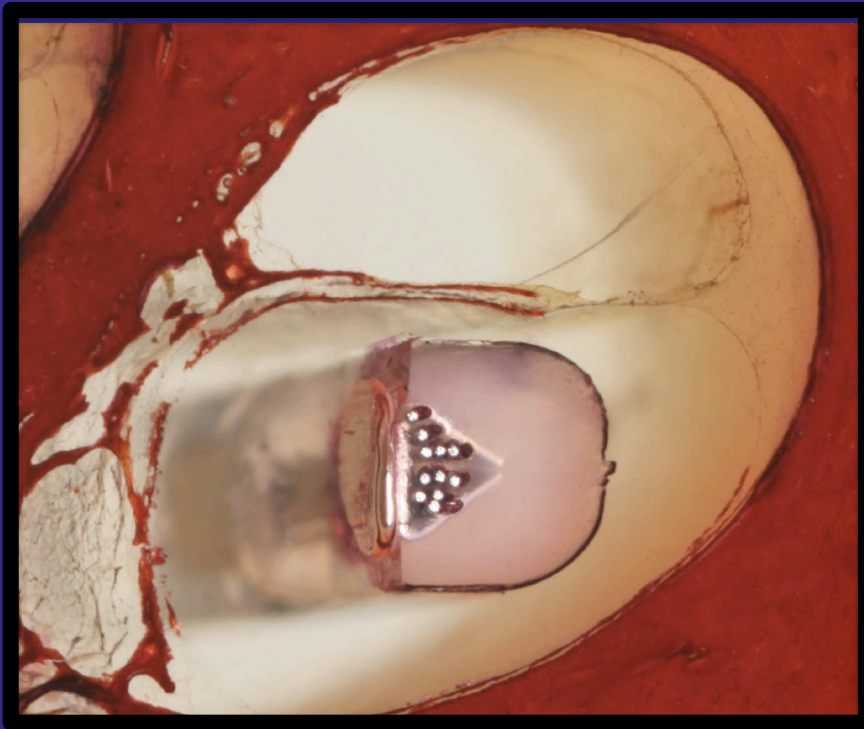


# Resulting change in rate of damage



Finley, et al

To be ultimately successful we need to combine the best electrode technology with optimum surgical technique.



How can we ensure this understanding is communicated in a meaningful way to surgeons worldwide?

Temporal bone insertions are excellent preparation for this clinical procedure.

Hospitals in China (n=19) practice with TBs ranged from 1- >40 per resident  
13 Hospitals = 5 or less, 6 Hospitals >10 TBs\*

\*Collaboration with Liu Shuai and Prof. Guan,  
Tsinghua University

# Summary

1. CI devices and subject performance are improving worldwide.
2. Cost of CI devices is declining and government support is increasing throughout the world. Nurotron will be a major part of this effort.
3. Supporting infrastructure, funding and training are key to broad access and quality of CI.



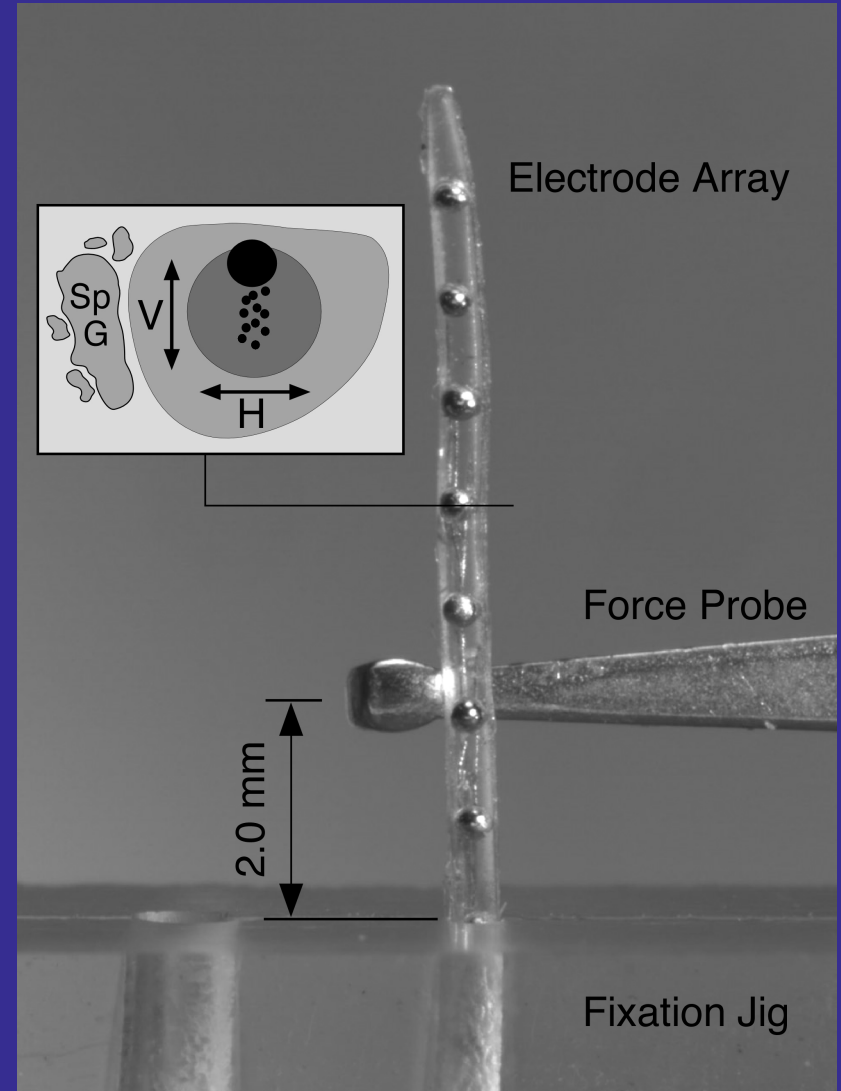
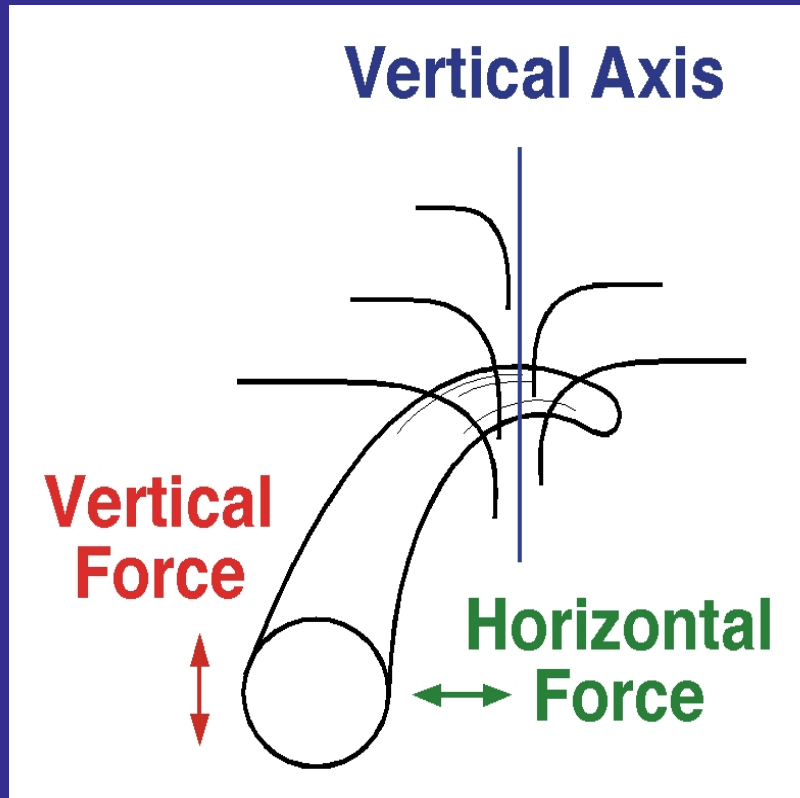
# Thank You



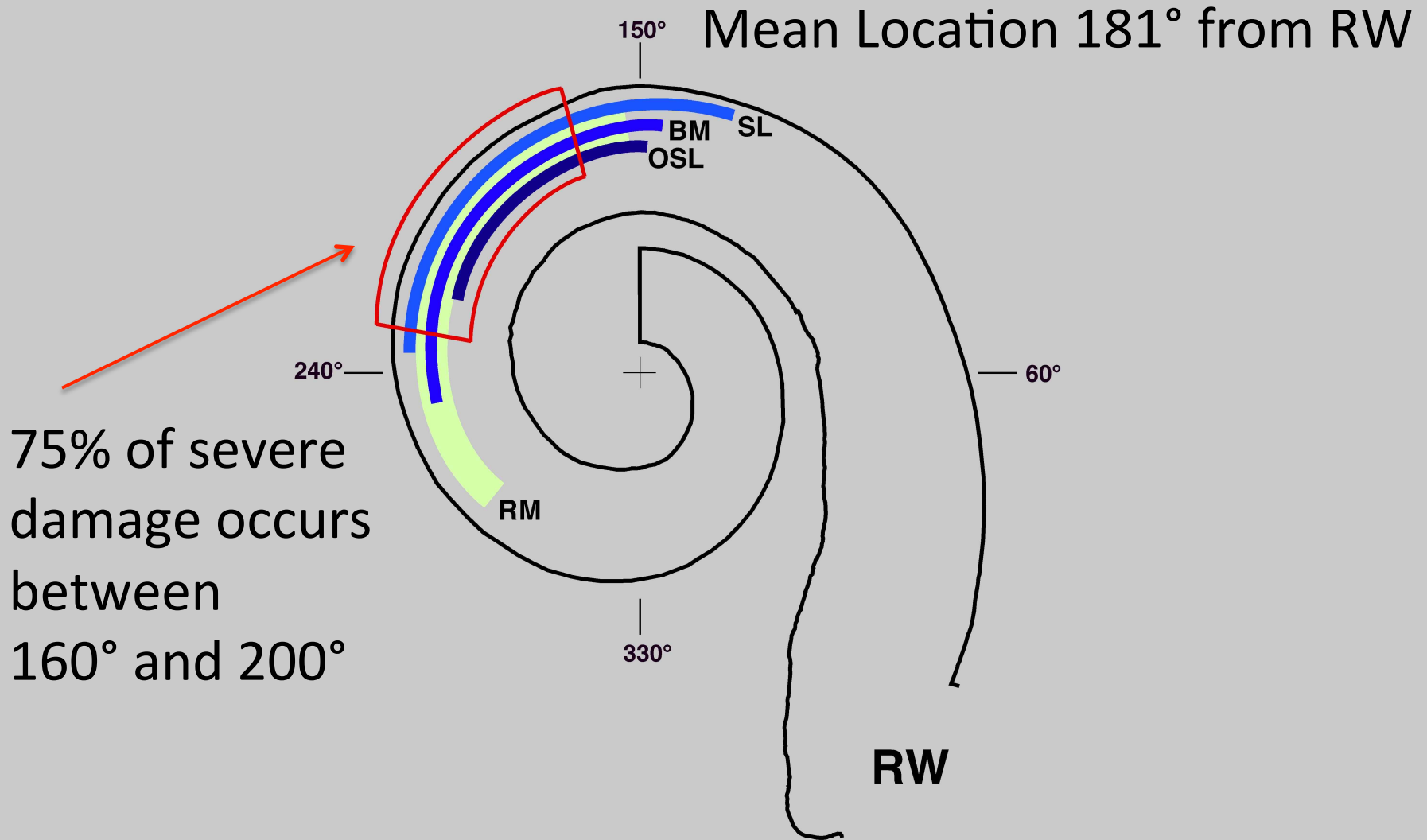


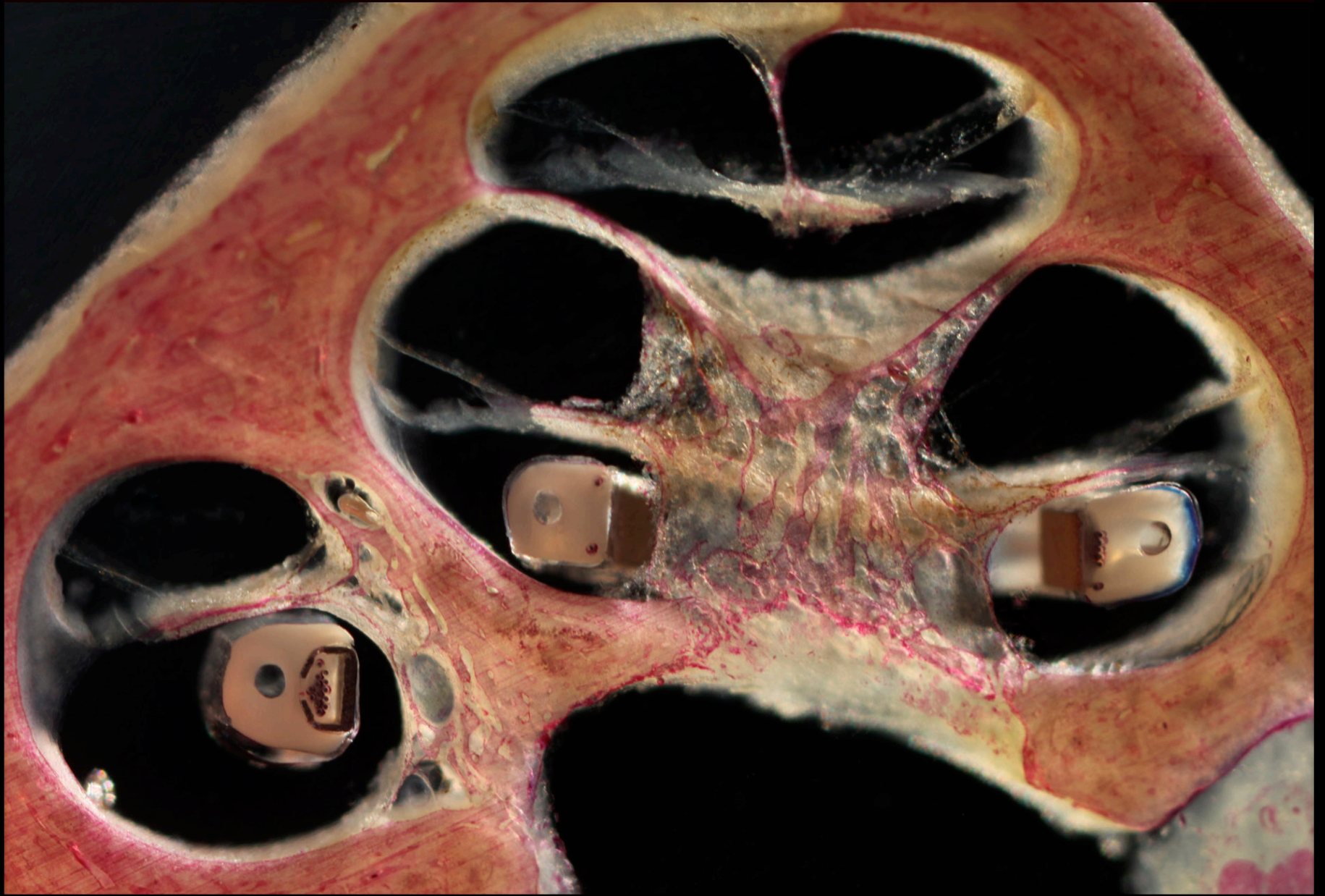


# How does electrode stiffness effect trauma?



Where, and how, does damage most often occur?



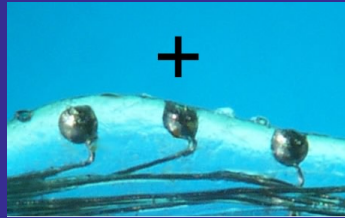


HiFocus Mid-Scala

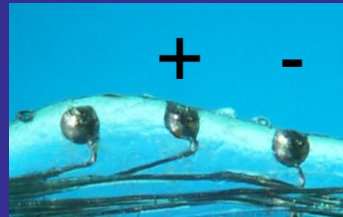
# Spread of excitation across the tonotopic gradient of the IC

*Future electrodes should have the capacity for greater numbers of channels.*

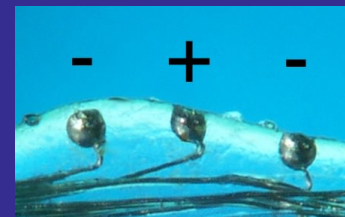
**Monopolar**



**Bipolar**



**Tripolar**



**Acoustic**

